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Angioplasty of arteries in the carotid territory.

J J Vitek

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cerebral vessels. Until such a trial has been performed, any statements about the relative usefulness of the two agents must be regarded as anecdotal (i.e., based on personal experience) and should not be construed as scientifically proved fact.

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Angioplasty of Arteries in the Carotid Territory

With regard to the article by Purdy et al. [1], for historical accuracy, I want to point out that S. A. Kadish, the head of endovascular surgery at the Latvian Medical Institute, Riga, U. S. S. R., has published many articles and presented numerous lectures on percutaneous transluminal angioplasty of the intracranial segment of the internal carotid artery and its branches. Dr. Kadish has performed more than 100 of these interventions, most of them on the internal and middle cerebral arteries. He uses special balloon angioplasty catheters of different sizes and shapes that he makes himself. He has had approximately 5% complications in a series of 100 patients.

His first articles on intracranial percutaneous transluminal angioplasty date back to 1982. Unfortunately, none of his papers were published outside the Soviet Union, and only a few of his lectures were presented in Western Europe or the United States. I have identified six of Dr. Kadish's publications related to intracranial percutaneous transluminal angioplasty, all of which were published in 1987-1990 in Riga (Latvia), Tallin (Estonia), Jerevan (Armenia), or Leningrad.

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Reply

I read with interest the letter from Dr. Vitek about the contribution of Dr. Kadish in the Soviet Union to the development of angioplasty techniques in arteries in the carotid territory. It comes as no surprise

that, with the history of interventional neuroradiology in the Soviet Union, scientists there have been involved in this area as well. Perhaps some of this work will be translated into English and become available to us to examine as to territories dilated, angiographic results, technical factors, and so forth. We might thus all benefit from Dr. Kadish's experiences. On the basis of Dr. Vitek's summary, I judge that such would be the case. Thanks to Dr. Vitek for pointing this out.

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Editor's Note.—The *American Journal of Neuroradiology* is a forum of international scope in neuroradiology. I certainly hope the thaw in East-West relations will prompt Dr. Kadish to share his experience in this emerging technology with his colleagues in Western Europe and North America. The Journal would welcome submission of such articles.

Xenon CT Scanning for Measurements of Cerebral Blood Flow

I read with interest the recent article by Good and Gur [1], who used computer simulations to evaluate the accuracy of cerebral blood flow (CBF) measurements made with xenon CT scanning. With the awareness that xenon itself alters CBF, the authors showed that for the particular protocol used in the computer model, the flow values calculated on the basis of a 5-min inhalation are not substantially affected by a 30-40% augmentation of CBF as long as the augmentation begins 1.5 min after the start of the study. Although this is certainly a step in the right direction, significant questions remain about the effect of xenon itself on flow values.

That xenon alters CBF has long been known, and recent work [2] has shown that velocities measured by using transcranial Doppler sonography change dramatically during the inhalation of xenon in concentrations commonly used for CT scanning. The velocities increased in 85% of a normal group 1.9 min after the onset of inhalation, rising to 38% above baseline levels. An augmentation of CBF induced by xenon has recently been confirmed by xenon-133 regional CBF studies [3]. In the computer simulation of Good and Gur, a corresponding behavior of CBF would not substantially affect the calculated flow values.

A problem with computer simulations is that specific simplifications must be assumed that ignore biological variability. For example, in the transcranial Doppler sonography study [2], 15% of the normal population showed a significant decrease in velocities in the middle cerebral arteries during xenon inhalation, in accordance with the known anesthetic effect of xenon. If xenon flow values are affected in a way suggested by these changes in blood-flow velocity, some subjects will show a small increase and some will show a small decrease in calculated flow values. The variability in these flow values that are due to the vasoactive effects of xenon can thereby be greatly magnified. Furthermore, the high variability of the time to onset of xenon flow activation (1.9 ± 0.56 min [SD]) implies an earlier activation for some patients than the 1.5-min constraint, which is critical in the computer model. The effects of the variability from either of these sources is not measured by the computer simulation of Good and Gur.

The situation is even worse for flow values of tissues that have pathologic changes. Although xenon reactivity and flow values of infarcted tissue are clearly zero, neither the magnitude nor the time course of xenon reactivity is known for living tissues with pathologic changes in the human brain. The amount of error due to xenon activation in these notoriously heterogeneous tissues is therefore completely unknown, and any xenon CT study of human tissue that

may seem to reflect pathophysiologic changes must be interpreted with great caution.

The numerous animal studies designed to correlate the results of xenon CT with the results of other techniques have not settled the issue. Many of these studies have used significantly higher concentrations of xenon or longer inhalation times than found in human protocols, so that the effect of xenon in these cases is unclear and, in fact, may decrease CBF. Furthermore, most of these studies have used only a handful of animals and have shown only a statistical correlation between xenon CT and other methods without addressing any actual agreement between the flow values. Systematic bias and high variability are therefore not reflected in the results, and many studies have reported a low correlation coefficient, which reflects a high variability. For example, analysis of graphic data found in a recent correlation study showed that 17 (57%) of 30 of the data points corresponded to xenon flow errors of more than 30%, despite good statistical correlation [4].

Animal studies are also confounded by the high variability in xenon reactivity between species, and results do not apply to human tissue. Unfortunately, despite tremendous anecdotal experience, we have no rigorous data that address the issue of flow value agreement in humans both for normal and for diseased brain.

Xenon CT scanning is a method of measuring CBF that itself changes flow, and so its quantitative use must be scrutinized. No computer simulation can capture the biological variability seen in the response times and magnitudes in a population, and no amount of parameter testing in a mathematical model can re-create the heterogeneous and largely unknown responses of diseased tissues to xenon. Although Good and Gur have shown a minimal effect of xenon in a restrictive computer model, they do not address these variabilities, nor do they address the significant proportion of xenon studies in which flow decreases. We have little knowledge of the effects of xenon on flow in human tissues with pathologic changes, and most of the correlative data are derived from small numbers of animals and show statistical correlation only. Because small changes in CBF in response to pharmacologic or physiologic changes are considered significant in clinical practice and in research, statistical correlation alone cannot suffice for clinical use. What is clearly needed is a quantitative comparison of flow values between xenon CT and a standard technique for both normal and abnormal tissue in humans. Although the xenon investigators should be applauded for having advanced xenon CT to a qualitative method for measuring CBF, the uncertainties mentioned here should prevent the acceptance of xenon CT as quantitative until such studies are performed.

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Reply

For several years, investigators and clinicians who used the xenon CT cerebral blood flow (CBF) washin protocol were puzzled by the

fact that consistent, robust, and reasonable flow values were routinely derived in such studies despite findings reported in the literature on CBF activation or deactivation during xenon inhalation [1]. The article by Giller et al. [1] states that "preliminary computer simulations assuming a rise in CBF during inhalation have confirmed the calculation of both significantly falsely high and low flow values for various choices of scanning times." Our results do not support this statement, nor did the results presented by Dr. Lindstrom, one of the coauthors of that article [1], during the International Conference on Stable Xenon/CT CBF in Orlando, FL, February 8-11, 1990 [2, 3].

We agree that significant alterations in flow may occur when xenon is inhaled at concentrations typically used in such studies. More importantly, these changes are likely to be patient-specific both in the time course and the amount of activation or deactivation. However, when appropriately selected scanning protocols are used for derivation of flow estimates, the resulting flow values quite accurately represent CBF at the time the study was started. We think that all three types of experiments—simulations, animal studies, and human studies—are important in this regard, and all three support the results we published based on simulation.

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Gadopentetate Dimeglumine-Enhanced MR Imaging of Spinal Dermal Sinus Tract

We read with interest the excellent article by Barkovich et al. [1] on MR evaluation of spinal dermal tracts in children. Recently, we saw a case of a spinal sinus dermal tract in which gadopentetate dimeglumine-enhanced MR imaging enabled us to make the correct diagnosis.

A 2-year-old boy had thoracic aplasia cutis congenita. Moving the head had always been painful. From the age of 16 months, the patient had had progressive neck pain and stiffness. He had had several episodes of high fever, and a subcutaneous abscess had developed at the level of T2, which had been treated surgically. Neurologic examination showed meningeal irritation and spasticity of both legs. Bladder and bowel functions were normal. Fever had abated, and CSF cultures were negative at this time.

Plain radiographs (not shown) of the thoracic spine showed fusion of the lamina of T1 and T2. MR imaging showed a dermal sinus tract at T3, seen as a linear structure of low signal intensity on sagittal T1-weighted images (Fig. 1A). The tract could be followed through the subcutaneous fat and posterior elements of the spine to the dura. The intraspinal portion of the tract was not visible. Gadopentetate dimeglumine-enhanced MR showed that the spinal tract ended in a soft-tissue mass with marked enhancement of signal intensity on T1-weighted images (Figs. 1B-1D). This soft-tissue mass extended caudally to the level of T5. Further MR examination of the entire spine did not show additional lesions, such as intra- or extradural tumors, thickened filum terminale, or abnormal position of the conus medullaris on images obtained before and after administration of gadopentetate dimeglumine.

The patient had dorsal laminectomy at the levels of T1 to T3. The